A Mathematical Theory of the Functional Dynamics of Cortical and Thalamic Nervous Tissue

H. R. Wilson and J. D. Cowan

1973

Gosse Overal



Spatial Temporal Model

Overview

- 1 Last presentation
- 2 Spatial Temporal Model
 - Descriptive Model
 - Simplification
 - Specification and Notes
- 3 Patterns
 - Active Transients
 - Spatially Localised Limit Cycles
 - Thalamic Oscilators
- 4 Conclusions



Recall:

Localized model neurons

Earlier work of Wilson and Cowan (1972). Excitatory (E) and inhibitory (I) neurons.

$$E(t+\tau) = \left(1 - \int_{t-r}^{t} E(t') dt'\right)$$

$$\cdot S_{e} \left(\int_{-\infty}^{t} \alpha(t-t') \left(c_{1}E(t') - c_{2}I(t') + P(t')\right) dt'\right)$$

$$I(t+\tau') = \left(1 - \int_{t-r}^{t} I(t') dt'\right)$$

$$\cdot S_{i} \left(\int_{-\infty}^{t} \alpha(t-t') \left(c_{3}E(t') - c_{4}I(t') + Q(t')\right) dt'\right)$$

Coarse Grained forms

$$\begin{split} &\tau\frac{\mathrm{d}\bar{E}}{\mathrm{d}t} = -\bar{E} + (1-r\bar{E})\mathcal{S}_{e}\left(kc_{1}\bar{E} - kc_{2}\bar{I} + kP\right) \\ &\tau'\frac{\mathrm{d}\bar{I}}{\mathrm{d}t} = -\bar{I} + (1-r\bar{I})\mathcal{S}_{i}\left(k'c_{3}\bar{E} - k'c_{4}\bar{I} + k'Q\right) \end{split}$$

Descriptive Model

Biological Context

- The authors compare the neural tissue of 3 species: Edible frog, Rabbit and Man.
- The higher vertibrates have more neurons and cortical surface.
- The thickness of cortex layers increases, but packing density decreases



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Patterns

- The thickness of cortex layers increases. but packing density decreases
- The number of neurons contained within a cylinder of cross sectional area of $1mm^2$ is roughly constant
- The authors postulate that: "individual anatomical regions of cerebral cortex are functinally organised as two-dimensional surfaces"
- and "One reason for the distribution of neurons in depth might be to provide the local redundancy necessary for reliable operation"



Goal: To model a very generalised cortex-like tissue

Assumptions:

- The cortical tissue is represented as a 2-D sheet.
- The cortical tissue consists of 2 types of neurons only, excitatory and inhibitory.
- The sheet is homogenous and isotropic i.e.
 - both types of neurons are uniformly distributed and
 - the lateral connectivity is dependent of distance only.
- Individual neurons summate incoming excitation both spatially and temporally, in a linear time-invariant fashion.
- Neurons have excitation thresholds θ and absolute refractory periods of duration r.
- There is a synaptic delay τ , i.e. the time between excitation reaching threshold and



1-D or 2-D?

The authors assume a 2-D sheet of cortical tissue.

Simplifying assumption

"Only stimuli that vary in one spatial dimension are considered" Homogeneity and isotropy imply patterns will only vary in the same dimension.

Assumption: Space is one dimensional.



Descriptive Model

Equations

Dependent variables: E(x,t), I(x,t)Independent variables: $t, x \in \mathbb{R}$

Mean rates of arrival of impulses at excitatory neurons

$$\begin{aligned} & \text{exc.:} \int_{-\infty}^{\infty} \varrho_e E\left(X, t - \frac{|x - X|}{v_e}\right) \beta_{ee}(x - X) \mathrm{d}X \\ & \text{inh.:} \int_{-\infty}^{\infty} \varrho_e I\left(X, t - \frac{|x - X|}{v_i}\right) \beta_{ie}(x - X) \mathrm{d}X \end{aligned}$$

And likewise for inhibitory neurons



Combine with external input and the post-synaptic membrane potential behaviour.

Mean value of excitation for excitable neuron at t, x:

Spatial Temporal Model

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$$N_{e}(x,t) = \int_{-\infty}^{t} \left(\int_{-\infty}^{\infty} \varrho_{e} E\left(X, T - \frac{|x - X|}{v_{e}}\right) \beta_{ee}(x - X) dX - \int_{-\infty}^{\infty} \varrho_{e} I\left(X, T - \frac{|x - X|}{v_{i}}\right) \beta_{ie}(x - X) dX \right)$$

$$\pm P(x, T) \alpha(t - T) dT$$

And likewise for inhibitory neurons



Finishing touches

Sensitive neurons

i.e. not refractory $R_e(x,t) = \left(1 - \int_{t-r_e}^{\infty} E(x,T) \mathrm{d}T\right) \varrho_e \delta x$

Descriptive Model

Finishing touches

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Expected number of activated neurons in interval δt

$$E(x, t + \tau)\varrho_e\delta x\delta t = R_e(x, t) \cdot S_e(N_e)\delta t$$

where ${\cal S}$ is the response function.

Descriptive Model

Hence we get

$$\begin{split} &E(x,t+\tau)\varrho_{e}\delta x\delta t \\ &= \left(1 - \int_{t-r_{e}}^{\infty} E(x,T)\mathrm{d}T\right)\varrho_{e}\delta x \cdot \mathcal{S}_{e} \bigg[\\ &\int_{-\infty}^{t} \left(\int_{-\infty}^{\infty} \varrho_{e}E\left(X,T - \frac{|x-X|}{v_{e}}\right)\beta_{ee}(x-X)\mathrm{d}X \\ &- \int_{-\infty}^{\infty} \varrho_{e}I\left(X,T - \frac{|x-X|}{v_{i}}\right)\beta_{ie}(x-X)\mathrm{d}X \\ &\pm P(x,T)\bigg)\alpha(t-T)\mathrm{d}T\bigg]\delta t \end{split}$$

And likewise for inhibitory neurons.

 ρ_e cancels and we let $\delta t, \delta x \to 0$.



We assume $\alpha(t)=\alpha e^{-\frac{t}{\mu}}$, where μ is the membrane time constant.

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Patterns

Further assumptions concerning simplification:

- Velocity of impulse propagation is very large compared to domain size.
- Use time coarse graining:

$$\langle E(x,t)\rangle = \frac{1}{\mu} \int_{-\infty}^{t} E(x,T) e^{-\frac{t-T}{\mu}} dT$$

and likewise for I, P and Q.

lacksquare $r_e \ll \mu$ and $au \ll \mu$

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and likewise for I, P and Q.

- $lap{r_e} \ll \mu$ and $au \ll \mu$
- Let ⊗ denote the convolution operation



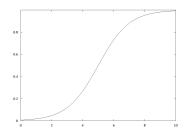
Simplified equations

$$\mu \frac{\partial}{\partial t} \langle E(x,t) \rangle = -\langle E(x,t) \rangle + (1 - r_e \langle E(x,t) \rangle)$$
$$\cdot \mathcal{S}_e[\alpha \mu (\varrho_e \langle E(x,t) \rangle \otimes \beta_{ee}(x)$$
$$-\varrho_i \langle I(x,t) \rangle \otimes \beta_{ie}(x) \pm \langle P(x,t) \rangle)]$$

$$\mu \frac{\partial}{\partial t} \langle I(x,t) \rangle = -\langle I(x,t) \rangle + (1 - r_i \langle I(x,t) \rangle)$$
$$\cdot S_i [\alpha \mu (\varrho_e \langle E(x,t) \rangle \otimes \beta_{ei}(x) - \varrho_i \langle I(x,t) \rangle \otimes \beta_{ii}(x) \pm \langle Q(x,t) \rangle)]$$

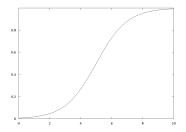
Specification and Notes

Recall: Sigmoid function



Recall:

Sigmoid function



Response function choice

$$\mathcal{S}_{\mathsf{e}}(\mathit{N}_{\mathsf{e}}) = \left(1 + e^{-
u(\mathit{N}_{\mathsf{e}} - \theta_{\mathsf{e}})}\right)^{-1} - \left(1 + e^{
u \theta_{\mathsf{e}}}\right)^{-1}$$



Exponentials are chosen for the connectivity function. The argument here is distance between two points (X - x)

$$\beta_{jj'}(x) = b_{jj'} e^{-|x|/\sigma_{jj'}}$$

Notes

Localized

Set the β functions constant (homogenous) over space.

This localized model exactly follows the model discussed last time for homogenous solutions.

non-linearity

The Partial differential integro formulae are very complex still. Analysis of behaviour and pattern formation is therefore done numerically by the authors.

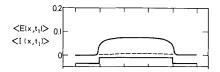


Apply stimulus in a block wave fashion

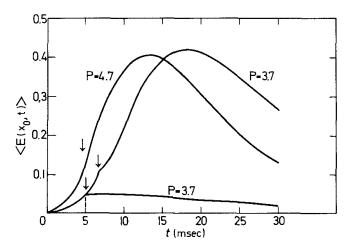
We apply the following:

$$\langle P(x,t)\rangle = \left\{ egin{array}{ll} 0 & ext{for} & x < L_1 \\ P & ext{for} & L_1 \le x \le L_2 \\ 0 & ext{for} & x > L_2 \end{array} \right.$$

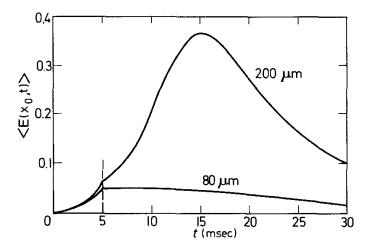
Length L, period Δt and signal strength P



Patterns 0•00

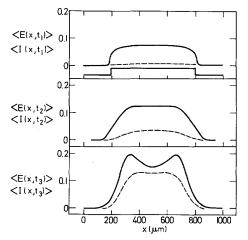




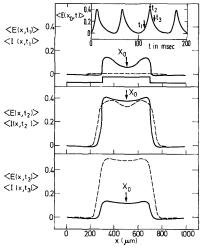




For even wider $L_2 - L_1$ we get edge inhancement:



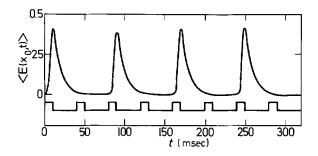
Apply sustained stimulus:



Patterns

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Summary of results

We conclude:

- Active transients can occur, but have a noise filter.
- Localised limit cycles can occur under sustained stimulus. The frequency increases monotonely with the stimulus.
- Thalamic Oscilators can also be modeled using this model. Frequency demultiplication can occur.

